
Compressed Sensing Microscopy with Scanning Line Probes

Anonymous Author(s)

Affiliation

Address

email

Abstract

1 In applications of scanning probe microscopy, images are acquired by raster
2 scanning a point probe across a sample. Viewed from the perspective of
3 compressed sensing (CS), this pointwise sampling scheme is inefficient,
4 especially when the target image is structured. While replacing point mea-
5 surements with delocalized, incoherent measurements has the potential to
6 yield order-of-magnitude improvements in scan time, implementing the
7 delocalized measurements of CS theory is challenging. In this paper we
8 study a partially delocalized probe construction, in which the point probe is
9 replaced with a continuous line, creating a sensor which essentially acquires
10 line integrals of the target image. We show through simulations, rudimen-
11 tary theoretical analysis, and experiments, that these line measurements
12 can image sparse samples far more efficiently than traditional point mea-
13 surements, provided the local features in the sample are enough separated.
14 Despite this promise, practical reconstruction from line measurements poses
15 additional difficulties: the measurements are partially coherent, and real
16 measurements exhibit nonidealities. We show how to overcome these limi-
17 tations using natural strategies (reweighting to cope with coherence, blind
18 calibration for nonidealities), culminating in an end-to-end demonstration.

19 1 Introduction

20 Scanning probe microscopy (SPM) is a fundamental technique for imaging interactions
21 between a probe and the sample of interest. Unlike traditional optical microscopy, the reso-
22 lution achievable by SPM is not constrained by the diffraction limit, making SPM especially
23 advantageous for nanoscale, or atomic level imaging, which has widespread applications in
24 chemistry, biology and materials science [1]. Conventional implementations of SPM typically
25 adopt a raster scanning strategy, which utilizes a probe with small and sharp tip, to form a
26 pixelated heatmap image via point-by-point measurements from interactions between the
27 probe tip and the surface. Despite their capability of nanoscale imaging, SPM with point-
28 wise measurement is inherently slow, especially when scanning a large area or producing
29 high-resolution images.

30 When the target signal is highly structured, compressed sensing (CS) [2, 3, 4] suggests it is
31 possible to design a data acquisition scheme in which the number of measurements is largely
32 dependent on the signal complexity, instead of the signal size, from which the signal can be
33 efficiently reconstructed algorithmically. In nanoscale microscopy, images are often spatially
34 sparse and structured. CS theory suggests for such signals, localized measurements such as
35 pointwise samples are inefficient. In contrast, delocalized, spatially spread measurements
36 are better suited for reconstructing a sparse image.

37 Unfortunately, the dense (delocalized) sensing
 38 schemes suggested by CS theory (and used in other
 39 applications, e.g., [5, 6, 7]) are challenging to im-
 40 plement in the setting of micro/nanoscale imaging.
 41 Motivated by these concerns, [8] introduced a new
 42 type of *semilocalized* probe, known as a *line probe*,
 43 which integrates the signal intensity along a straight
 44 line, and studied it in the context of a particular mi-
 45 croscopy modality known as scanning electrochemi-
 46 cal microscopy (SECM) [9, 10]. In SECM with *line*
 47 *probe*, the working end of the probe constitutes a straight line, produces a single measurement
 48 by collecting accumulated redox reaction current induced by the probe and sample. These
 49 line measurements are semilocalized, samples a spatially sparse image more efficiently than
 50 measurements from point probes, and “has an edge” on high resolution imaging since a thin
 51 and sharp line probe can be manufactured with ease. Moreover, experiments in [8] suggest
 52 that a combination of line probes and compressed sensing reconstruction could potentially
 53 yield order-of-magnitude reductions in imaging time for sparse samples.

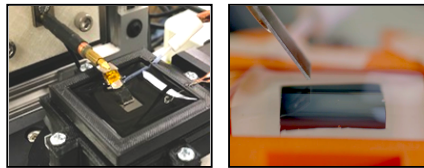


Figure 1: Left: lab made SECM device with line probe. Right: closeup side view of line probe near a sample surface.

54 Realizing the promise of line probes (both in SECM and in microscopy in general) demands
 55 a more careful study of the mathematical and algorithmic problems of image reconstruction
 56 from line scans. Because these measurements are structured, they deviate significantly
 57 from conventional CS theory, and basic questions such as the number of line scans required
 58 for accurate reconstruction are currently unanswered. Moreover, practical reconstruction
 59 from line scans requires modifications to accommodate nonidealities in the sensing system.
 60 In this paper, we will address both of these questions through rudimentary analysis and
 61 experiments, showing that if the local features are either small or separated, then stable
 62 image reconstruction from line scans is attainable.

63 1.1 Related work

64 **Compressed sensing tomography.** Line measurements also arise in *computational tomogra-*
 65 *phy* (CT) imaging [11, 12, 13, 14, 15, 16]. Classical CT reconstruction recovers an image from
 66 densely sampled line scans, by approximately solving an inverse problem [17, 18]. These
 67 methods do not incorporate the prior knowledge of the structure of the target image, and
 68 degrade sharply when only a few CT scans are available. Compressed sensing offers an
 69 attractive means of reducing the number of measurements needed for accurate CT image
 70 reconstruction, and has been employed in applications ranging from medical imaging to
 71 (cryogenic) electron transmission microscopy [19, 20, 21, 22, 23, 24, 25, 26]. The dominant
 72 approach assumes that the target image is sparse in a Fourier or wavelet basis, and recon-
 73 structs it via ℓ^1 minimization or related techniques. Images in SECM and related modalities
 74 typically exhibit much stronger structure: they often consist some number of small particles
 75 [27, 28], or other repeated motifs [29]. In this situation, CS is especially promising. On the
 76 other hand, as we will see below, understanding the interaction between line scans and
 77 spatially localized features demands that we move beyond conventional CS theory.

78 **Mathematical theory of line scans: Radon transform and image super-resolution.** The
 79 question of recoverability from line measurements is related to the theory of the *Radon*
 80 *transform*, which corresponds to a limiting situation in which line scans at every angle are
 81 available [30, 31, 32]. The Radon transform is invertible, meaning perfect reconstruction is
 82 possible (albeit not stable) in this limiting situation. Due to the *projection slice theorem* [33],
 83 the line projections are inherently lowpass, and so the line scan reconstruction problem is
 84 related to superresolution imaging [34]. When the image of interest consists of sparse point
 85 sources, the image can be stably recovered from its low-frequency components, provided the
 86 point sources are sufficiently separated [35]. Similarly, we can hope to achieve stable recovery
 87 of localized features from line scans as long as the features are sufficiently separated.

88 2 Line measurement model

89 To implement line scans for SECM, a line probe (Figure 1) is mounted on an automated
 90 arm which positions the probe onto the sample surface. The line scan signal is generated by
 91 placing this line probe in different places, and measuring the integrated current induced by
 92 the interaction between the line probe and the electroactive part of the sample. In a pragmatic

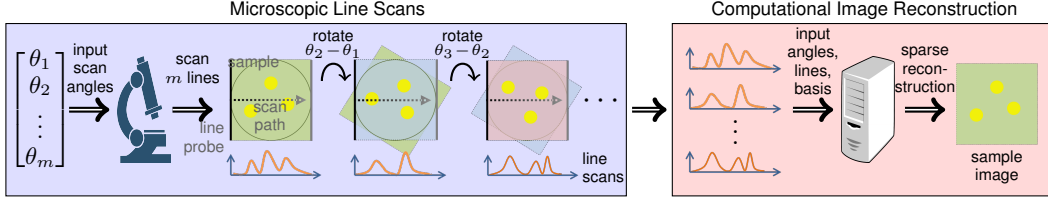


Figure 2: Flow chart for scanning procedure of SECM with continuous line electrode probe.

93 scanning procedure (Figure 2), the user will choose distinct scanning angles $\theta_1, \dots, \theta_m$. For
 94 each angle θ , the line probe is oriented in direction $\mathbf{u}_\theta = (\cos \theta, \sin \theta)$ and swept along the
 95 normal direction $\mathbf{u}_\theta^\perp = (\sin \theta, -\cos \theta)$. Each sweep of probe generates the projection of the
 96 target image along the probe direction \mathbf{u}_θ ; collecting these projections for each θ_i , we obtain
 97 our complete set of measurements.

98 **Line projection.** To describe the scanning procedure more precisely, we begin with a
 99 mathematical idealization, in which the probe measures a line integral of the image. In this
 100 model, when the probe body is oriented in direction \mathbf{u}_θ at position t , we observe the integral
 101 of the image over $\ell_{\theta,t} := \{\mathbf{w} \in \mathbb{R}^2 \mid \langle \mathbf{u}_\theta^\perp, \mathbf{w} \rangle = t\}$:

$$\mathcal{L}_\theta[\mathbf{Y}](t) := \int_{\ell_{\theta,t}} \mathbf{Y}(\mathbf{w}) d\mathbf{w} := \int_s \mathbf{Y}(s \cdot \mathbf{u}_\theta + t \cdot \mathbf{u}_\theta^\perp) ds. \quad (2.1)$$

102 Collecting these measurements for all t , we obtain a function $\mathcal{L}_\theta[\mathbf{Y}]$ which is the projection
 103 of the image along the direction \mathbf{u}_θ . We refer to the operation $\mathcal{L}_\theta : L^2(\mathbb{R}^2) \rightarrow L^2(\mathbb{R})$ as a
 104 *line projection*. Combining projections in m directions $\Theta = \{\theta_i\}_{i=1}^m$, we obtain an operator
 105 $\mathcal{L}_\Theta : L^2(\mathbb{R}^2) \rightarrow L^2(\mathbb{R} \times [m])$:

$$\mathcal{L}_\Theta[\mathbf{Y}] := \frac{1}{\sqrt{m}} [\mathcal{L}_{\theta_1}[\mathbf{Y}], \dots, \mathcal{L}_{\theta_m}[\mathbf{Y}]]. \quad (2.2)$$

106 **Line scans.** In reality, it is not possible to fabricate an infinitely sharp line probe, and hence
 107 our measurements do not correspond to ideal line projections, but rather their convolution
 108 with a point spread function ψ that models blurring along the scanning direction. In SECM,
 109 ψ is typically skewed, with a long tail in the sweeping direction. Accounting for this effect
 110 is important, if we wish to obtain accurate reconstructions in practice. In this more realistic
 111 model, our measurements become

$$\tilde{\mathbf{R}} = \frac{1}{\sqrt{m}} [\psi * \mathcal{L}_{\theta_1}[\mathbf{Y}], \dots, \psi * \mathcal{L}_{\theta_m}[\mathbf{Y}]] =: \psi * \mathcal{L}_\Theta[\mathbf{Y}]. \quad (2.3)$$

112 This measurement consists of m functions $\psi * \mathcal{L}_{\theta_i}[\mathbf{Y}](t)$ of a single (real) variable t , which
 113 corresponds to the translation of the probe in the $\mathbf{u}_{\theta_i}^\perp$ direction. In practice, we do not measure
 114 this function at every t , but rather collect n equispaced samples, giving measurements
 115 $\mathbf{R}_i = \mathcal{S}\{\tilde{\mathbf{R}}_i\} \in \mathbb{R}^n$ and $\mathbf{R} = [\mathbf{R}_1, \dots, \mathbf{R}_m] \in \mathbb{R}^{n \times m}$. Our task is to understand when and
 116 how we can reconstruct the target image \mathbf{Y} from these samples.

117 3 Promises and problems of line scans

118 3.1 Compressed sensing of line projections for highly localized image

119 As a proof of concept, we first show that the line probe can efficiently sense sparse images
 120 consisting of well-separated features:

121 **Lemma 3.1.** Consider an image consists of $k \geq 2$ discs radius r . If the centers $\mathbf{w}_1, \dots, \mathbf{w}_k$ are
 122 separated such that $\min_{i \neq j} \|\mathbf{w}_i - \mathbf{w}_j\|_2 > \frac{2}{C} k^2 r$, then three line scans with probe direction chosen
 123 independent uniformly at random suffice to recover the image with probability at least $1 - C$.

124 Lemma 3.1 shows if we assume the sparse component of the image signal are small and
 125 separated discs; if the radius of the discs are sufficiently small, then, perhaps surprisingly,
 126 only three line projections are required to exactly reconstruct the image.

127 3.2 Reconstructability from line projections of localized image in practice

128 While the microscopic images are often sparse in spatial domain, they rarely satisfy the
 129 conditions of Lemma 3.1. In the following, we show that in practical application of line scans,
 130 when the image consists of multiple localized motifs, the performance of line measurements
 131 degrades as the ratio between the size of motifs and their separation increases.

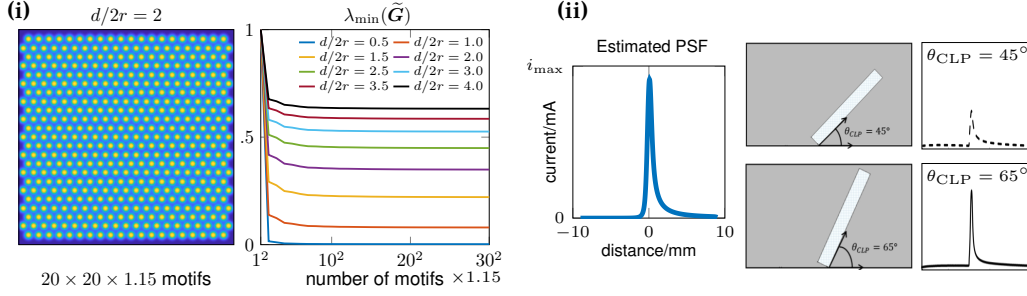


Figure 3: (i): Least eigenvalue of $\tilde{\mathbf{G}}$ with motifs on hexagonal lattice. We show an example image of motifs placed on the lattice locations (left), and calculate the least eigenvalue with varying number of motifs and distance-to-diameter ratio (right). (ii): The point spread function of line probe is skewed in the sweeping direction. We show a close form PSF used for reconstruction (left); and software (LabVIEW) simulated PSF whose shape and intensity changes as the contacting angle varies (right).

132 **Coherence of line projection of two localized motifs** Inspired by CS, we study the con-
 133 ditioning of the line projection \mathcal{L}_Θ when it is restricted to an image with sparsely populated
 134 motifs $\mathbf{D} \in L^2(\mathbb{R}^2)$. Consider an image with two motifs located at different locations, and
 135 define a 2×2 Gram matrix \mathbf{G} with its ij -th entries being *coherence* [36] between line projected
 136 signal of two motifs \mathbf{D} with center at \mathbf{w}_i and \mathbf{w}_j respectively,

$$\mathbf{G}_{ij} = \langle \mathcal{L}_\Theta[\mathbf{D} * \delta_{\mathbf{w}_i}], \mathcal{L}_\Theta[\mathbf{D} * \delta_{\mathbf{w}_j}] \rangle. \quad (3.1)$$

137 If the off-diagonal entry \mathbf{G}_{ij} is small in magnitude compared to the diagonal entries $\mathbf{G}_{ii}, \mathbf{G}_{jj}$,
 138 then it suffices to reconstruct the image exactly with efficient algorithm. Conversely, if \mathbf{G} is
 139 ill-conditioned or even rank-deficient, then exact recovery will be impossible.

140 **Lemma 3.2.** *Let \mathbf{D} be a two-dimensional Gaussian pdf with variance r and normalized in a sense*
 141 *that $\|\mathcal{L}_0[\mathbf{D}]\|_{L^2} = 1$. If θ is uniformly random, then the expectation of inner product between two*
 142 *line projected \mathbf{D} at different locations $\mathbf{w}_i, \mathbf{w}_j$ is bounded by*

$$\left(1 - \frac{d^2}{8r^2}\right) \mathbf{1}_{d \leq 2r} + \frac{r}{2d} \mathbf{1}_{d > 2r} \leq \mathbb{E}_\theta \langle \mathcal{L}_\theta[\mathbf{D} * \delta_{\mathbf{w}_i}], \mathcal{L}_\theta[\mathbf{D} * \delta_{\mathbf{w}_j}] \rangle \leq \frac{1}{\sqrt{1 + d^2/4r^2}}. \quad (3.2)$$

143 where $d = \|\mathbf{w}_i - \mathbf{w}_j\|_2$ and $\delta_{\mathbf{w}}$ is the Dirac measure at \mathbf{w} .

144 **Lemma 3.2** shows the coherence between line projections of two Gaussian of variance r
 145 and center distance d is dominated by the distance-to-diameter ratio $d/2r$. Because of the
 146 projection slice theorem, the matrix $\mathbb{E}_\theta \mathbf{G}$ is always positive definite. However, its condition
 147 number greatly increases when the image consists of highly overlapping local features.
 148 When the ratio is small, say $d/2r < 1$, in which the two projected motifs are overlapping, then
 149 $\mathbb{E}_\theta \mathbf{G}_{ij}$ will be close to one as with the diagonals, implies $\mathbb{E}_\theta \mathbf{G}$ become severely ill-conditioned
 150 even in the two-sparse case. Generally speaking, line scans are not CS-theoretical optimal
 151 sampling method for sparse recovery for image of superposing discs.

152 **Injectivity of line projection of multiple motifs with minimum separation** To extend
 153 the study of the coherence of matrix \mathbf{G} to samples that contain $k > 2$ motifs \mathbf{D} . We first
 154 investigate a model configuration whose motif centers are allocated on a hexagonal lattice
 155 with edges of length d . It turns out that the smallest eigenvalue of an approximation \mathbf{G} with
 156 respect to the locations $\{\mathbf{w}_1, \dots, \mathbf{w}_k\}$ is largely determined by the distance-to-diameter ratio
 157 $d/2r$, and depends only weakly on the total number of motifs.

158 In **Figure 3**, we calculate the least eigenvalue of an approximation $\mathbb{E}_\theta \mathbf{G}$ with $\tilde{\mathbf{G}}$, where
 159 $\tilde{\mathbf{G}}_{ij} = (1 + \|\mathbf{w}_i - \mathbf{w}_j\|_2^2 / 4r^2)^{-1/2}$ is obtained from the upper bound in **Lemma 3.2**. We show
 160 that when these motifs are highly overlapping with distance-to-diameter ratio $d/2r = 0.5$,
 161 the least eigenvalue of $\tilde{\mathbf{G}}$ is very close to zero and the matrix is nearly rank-deficient; when
 162 the motifs are separated, say $d/2r \geq 1$, the least eigenvalue of $\tilde{\mathbf{G}}$ is steadily larger than
 163 zero and approaches one as the ratio $d/2r$ increases. Interestingly, in our experiments
 164 the least eigenvalue does not depend strongly on the number of motifs, suggesting that
 165 the distance-to-diameter ratio is the dominant factor for injectivity of line projections on
 166 motifs with hexagonal placement. Since the hexagonal configuration is the densest circle

167 packing on a plane, we suspect that $\lambda_{\min}(\mathbb{E}_\theta \mathbf{G})$ is also determined by the ratio $d/2r$ for every
 168 configurations satisfying the minimum separation property. This conjecture gains more
 169 ground when viewing this problem from the point source super-resolution perspective [35].
 170 It is known that an image consisting of point measures $\mathbf{x} = \sum_i \alpha_i \delta_{\mathbf{w}_i}$ can be stably recovered
 171 from its low frequency information (with frequency cutoff f_c) whenever the point sources
 172 have minimum separation $d > C/f_c$ for some constant C , regardless of the number of such
 173 point measures in \mathbf{x} . In our scenario, we will show that the expected line projection $\mathbb{E}_\theta \mathcal{L}_\theta^* \mathcal{L}_\theta$
 174 is also a low-pass filter; and since the local features \mathbf{D} is also often consists of low frequency
 175 components, our line projections $\mathcal{L}_\theta[\mathbf{D} * \mathbf{X}]$ can be modeled as the low-pass measurements
 176 from sparse map \mathbf{X} , implying stable and efficient sparse reconstruction is possible as long
 177 as \mathbf{X} is enough separated under infinitely many line measurements of all angles.

178 **Lemma 3.3.** *Suppose \mathbf{D} is two-dimensional Gaussian of variance r with $\|\mathcal{L}_0[\mathbf{D}]\|_{L^2} = 1$ and \mathbf{X} is
 179 finite summation of Dirac measure. If θ is uniformly random, then $\mathbb{E}_\theta \mathbf{D} * \mathcal{L}_\theta^* \mathcal{L}_\theta[\mathbf{D} * \mathbf{X}]$ is a lowpass
 180 filter \mathcal{K} on \mathbf{X} with cut-off frequency f_c satisfying*

$$f_c = \frac{1}{r} \cdot \min \left\{ 2r^2 \varepsilon^{-1}, \sqrt{|\log(8r^2 \varepsilon^{-1})|} + 0.2 \right\}, \quad (3.3)$$

181 *in the sense that $\max_{\|\boldsymbol{\xi}\|_2 \geq f_c} |\mathcal{F}_2\{\mathcal{K}\}(\boldsymbol{\xi})| \leq \varepsilon$.*

182 **Lemma 3.3** shows when the radius of \mathbf{D} is sufficiently large, then the cut-off frequency f_c is
 183 dominated by the cut-off frequency of \mathbf{D} , hence it is sufficient to recover \mathbf{X} as long as the
 184 separation d satisfies $d > Cr$, which is also reflected from the observation of [Figure 3](#). In cases
 185 with small (pointy) \mathbf{D} , the cut-off frequency is mainly determined by the low-pass property
 186 of line projection, which requires minimum separation $d > C\varepsilon/r$ for exact reconstruction.

187 3.3 Obstacles of image reconstruction from line scans

188 Besides the apparent nonideality of coherence of line scan measurements which is not
 189 CS theoretical optimal, this specific sampling method and its corresponding hardware
 190 limitations causes other practical nuisances during image reconstruction.

191 **High coherence of line scans.** To show the coherence is a cause for concern, consider the
 192 nonnegative Lasso

$$\min_{\mathbf{X} \geq 0} \lambda \|\mathbf{X}\|_1 + \frac{1}{2} \|\mathbf{A}[\mathbf{X}] - \mathbf{R}\|_2^2 \quad (3.4)$$

193 from observstion $\mathbf{R} = \mathbf{A}[\mathbf{X}_0]$ and linear, column normalized and coherent sampling method
 194 \mathbf{A} . Denote Ω as the support set of solution of (3.4), write \mathbf{A}_Ω as the submatrix of \mathbf{A} restricted
 195 on columns of support Ω , the unique solution \mathbf{X} of program (3.4) (provided if \mathbf{A}_Ω is injective)
 196 can be written as

$$\mathbf{X}_{ij} = [\mathbf{X}_{0ij} - \lambda(\mathbf{A}_\Omega^* \mathbf{A}_\Omega)^{-1} \mathbf{1}]_+ \quad \mathbf{w}_{ij} \in \Omega; \quad \mathbf{X}_{ij} = 0 \quad \mathbf{w}_{ij} \notin \Omega. \quad (3.5)$$

197 When \mathbf{A} is coherent, columns of \mathbf{A} have large inner product, implies many entries of the
 198 matrix $\mathbf{A}_\Omega^* \mathbf{A}_\Omega$ have large, positive off-diagonal entries close to its diagonals. When the sparse
 199 penalty λ is large in (3.4), its solution will have incorrect relative magnitudes since $\mathbf{A}_\Omega^* \mathbf{A}_\Omega$
 200 is not close to identity matrix as conventional CS measurements [37]. When λ is small, the
 201 solution of program will be highly sensitive to noise, occasionally leading to incorrect results.

202 **Incomplete information of PSF of line scans.** Another layer of complexity for CLP scans
 203 is the difficulty to correctly identify its PSF due to hardware limitations, especially when
 204 operating line scans in nanoscale. For instance in [Figure 3](#) (right), we show if the contacting
 205 angle between the probe and the sample varies, the corresponding PSF changes drastically
 206 in both the peak magnitude and the shape. It turns out that even with seemingly small
 207 changes of probe condition, the corresponding PSF can be inevitably varied.

208 4 Reconstruction from line scans

209 In all following experiments, we consider a representative class of images \mathbf{Y} characterized
 210 by superposing reactive species \mathbf{D} at locations $\mathcal{W} = \{\mathbf{w}_1, \dots, \mathbf{w}_{|\mathcal{W}|}\} \subset \mathbb{R}^2$ with intensities
 211 $\{\alpha_1, \dots, \alpha_{|\mathcal{W}|}\} \subset \mathbb{R}_+$. Define the activation map \mathbf{X}_0 as sum of Dirac measure at \mathcal{W} , then \mathbf{Y}
 212 can simply be written as convolution between \mathbf{D} and \mathbf{X}_0 :

$$\mathbf{Y} = \mathbf{D} * \mathbf{X}_0 = \sum_{j=1}^{|\mathcal{W}|} \alpha_j \mathbf{D} * \delta_{\mathbf{w}_j}. \quad (4.1)$$

213 The image reconstruction problem is then cast as finding the best fitting sparse map $\widehat{\mathbf{X}}$
 214 from line scans $\mathbf{R} = \mathcal{S}\{\Psi * \mathcal{L}_\theta[\mathbf{Y}]\}$, and the reconstructed image is simply $\mathbf{D} * \widehat{\mathbf{X}}$. Since all

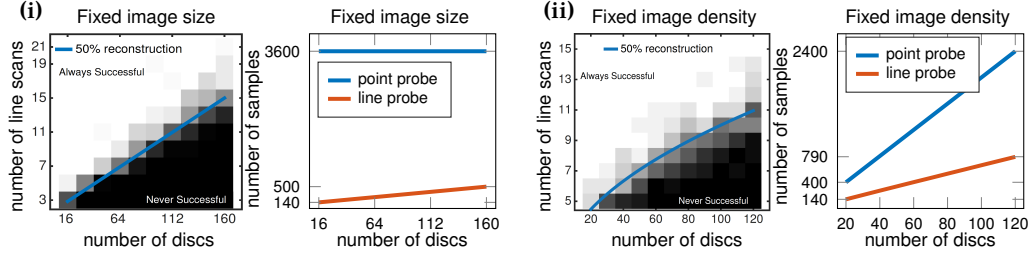


Figure 4: Phase transition [8] of fixed image size (i) and fixed density (ii) on support recovery with Lasso. In all experiments $d/2r \geq 1$ is ensured. Both of the phase transitions show the number of line scans required is almost linear proportional to the number of discs for exact reconstruction, and the scanning efficiency is better than point probe by 3-10 times.

215 associated operations on X_0 (convolution with D , ψ and line projection \mathcal{L}_Θ) are all linear,
 216 this becomes a sparse estimation problem, which can be solved via the Lasso:

$$\min_{\mathbf{X} \geq 0} \lambda \sum_{ij} \mathbf{X}_{ij} + \frac{1}{2} \|\mathbf{R} - \mathcal{S}\{\psi * \mathcal{L}_\Theta[D * \mathbf{X}]\}\|_2^2. \quad (4.2)$$

217 4.1 Sparse recovery with Lasso from line projections

218 In light of Section 3.2, the measurement performance using infinitely many line scans is
 219 almost dependent only on the distance-to-diameter ratio of the local features. Since in
 220 practice, only finite number line scan is available, we want to study how many line scans
 221 will be sufficient for efficient and exact sparse image reconstruction. We do this by studying
 222 the performance of algorithm (4.2) while assuming the line scan are idealized where $\psi = \delta$.

223 Figure 4 shows the reconstruction performance from line scans with varying number of
 224 line scans (uniform randomly chosen angle) used and number of discs in the images \mathbf{Y}
 225 (discs of radius r at random location satisfying $d/2r \geq 1$ via rejection sampling). Here, two
 226 experiment setting is presented: fixed area ($3 \times 3 \text{mm}^2$, disc radius $50 \mu\text{m}$) and fixed density (20
 227 discs/ mm^2 , disc radius $50 \mu\text{m}$). In the phase transition (PT) image, each pixel represents
 228 the average of 50 experiments; and in each experiment, given a random image \mathbf{Y} line scans,
 229 if solving (4.2) correctly identify the support map of \mathbf{Y} , then the algorithm succeeds, and
 230 vice versa. It shows clear transition lines in both PT images, and the comparison of scanning
 231 time between line/point probes shows clear improvement of scanning efficiency.

232 Interestingly if we compare the result with CS theory, which asserts the number measurement
 233 of samples required is close to linear proportional to signal sparsity; here, though the line
 234 scans are not CS-optimal, both PT images exhibits similar phenomenon. When the image
 235 size is fixed, total number of samples m is proportional to the line scan count N , with PT
 236 transition line showing linear proportionality between number of line scans and discs $N \propto k$,
 237 gives $m \propto k$; on the other hand, when the image density is fixed, the number of samples m
 238 is proportional to $N \times \sqrt{k}$ while the transition line in PT is showing $N \propto \sqrt{k}$, again suggests
 239 linear proportionality between number of measurement and sparsity $m \propto N\sqrt{k} \propto k$.

240 In either case, line measurements are substantially more efficient than measurements with a
 241 point probe. Realizing this gain in practice requires us to modify the Lasso to cope with the
 242 following nonidealities: (i) line scans are coherent, (ii) the PSF ψ is typically only partially
 243 known, and (iii) naive approaches to computing with line scans are inefficient when the
 244 target resolution is large. Below, we show how to address these issues, and give a complete
 245 reconstruction algorithm.

246 4.2 Practical Reconstruction with Nonidealities

247 **Fast computation of discrete line projection** The line projection of an image \mathbf{Y} in direction
 248 of angle θ is equivalent to the line projection at 0° of clockwise rotated \mathbf{Y} by angle θ .
 249 This enables an efficient line projection computationally via fast image rotation with shear
 250 transform in Fourier domain [38] (see appendix); and more importantly, its adjoint (back
 251 projection) can be computed in a similarly explicit manner.

252 **Reweighting Lasso for coherent measurements** To cope with the coherence phenomenon,
 253 we adopt the reweighting scheme [39] by solving Lasso formulation (4.2) multiple times

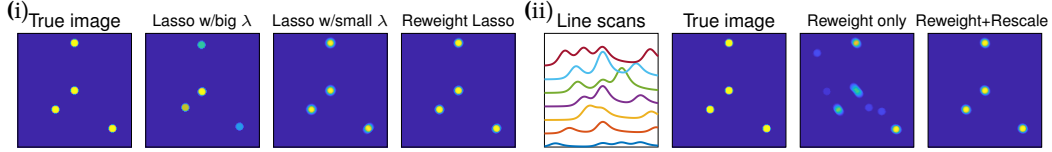


Figure 5: (i). To reconstruct the image (left) from 6 line scans with simulated PSF in Figure 3 using Lasso with large λ gives images of unbalanced magnitude (mid left) due to coherence; while using Lasso with small λ provides blurry image (mid right) due to the weakened sparsity regularizer. Reweighted Lasso (right) consistently generates good result. (ii). We simulate a line scan with uneven magnitude (left) from image (mid left). Reweighting method (mid right) cannot identify the correct support; while the reweighting plus calibration method (right) approximately recovers the image.

254 while updating penalty variable λ in each iterate. At k -th iterate, the algorithm chooses the
 255 regularizer λ in (4.2) base on the previous outcome of lasso solution $\mathbf{X}^{(k)}$, where

$$\lambda_{ij}^{(k)} \leftarrow C(\mathbf{X}_{ij}^{(k-1)} + \varepsilon)^{-1} \quad (4.3)$$

256 with ε being the machine precision constant and C being close to the smooth part in (4.2). The
 257 effect of reweighting method is two-fold: (i) it is a majorization-minimization algorithm of
 258 sparse regression using log-norm as sparsity surrogate [39], hence, discovers sparse solution
 259 more effectively compares to the use of ℓ^1 -norm in Lasso; and (ii) the sparsity surrogate in

260 final stages of reweighting approaches ℓ^0 -norm, by seeing $\frac{\mathbf{X}_{ij}^{(k+1)}}{\mathbf{X}_{ij}^{(k)} + \varepsilon} \approx 1$ if $\mathbf{X}_{ij}^{(k)} \neq 0$ as $k \rightarrow \infty$.

261 As a result, in the final stages, problem (4.2) effectively turns into least squares, restricted
 262 to the support of \mathbf{X} , which produces a sparse solution with correct magnitude. Figure 5
 263 (left) displays an example of reweighting scheme, showing better reconstruction result than
 264 vanilla Lasso.

265 **Blind calibration for incomplete PSF information** We can cope with incomplete infor-
 266 mation about the PSF by working with a parametric family of PSF's and optimizing the
 267 parameters at reconstruction time. Here, we allow the PSF to vary from scan to scan, writing
 268 $\psi(\mathbf{p}_i)$ for the PSF for the i -th scan, with parameters \mathbf{p}_i . We optimize both the parameters
 269 $\mathbf{p}_1 \dots \mathbf{p}_m$ and the sparse map \mathbf{X} via alternating minimization. Figure 5 (right) exhibits a
 270 simulated example in which the PSF of line scans has unbalanced magnitudes due to the
 271 variation of probe scanning angle (Figure 3), suggests incorporating calibration scheme
 272 achieves successful reconstruction while non-calibration method falls short.

273 4.3 Image reconstruction algorithm from line scans

274 Finally we formally state the complete algorithm (see appendix) for reconstruction of SECM
 275 image from its line scans. The algorithm solves multiple iterations of

$$\min_{\mathbf{X} \geq 0, \mathbf{p} \in \mathcal{P}} \sum_{ij} \lambda_{ij}^{(k)} \mathbf{X}_{ij} + \sum_{i=1}^m \frac{1}{2} \|\mathcal{S}\{\psi(\mathbf{p}_i) * \mathcal{L}_{\theta_i}[\mathbf{D} * \mathbf{X}]\} - \mathbf{R}_i\|_2^2. \quad (4.4)$$

276 while updating the penalty variable $\lambda^{(k)}$ in each iterate base on (4.3) with $C \approx \frac{1}{2} \|\mathcal{S}\{\psi * \mathcal{L}_{\Theta}[\mathbf{D} * \mathbf{X}^{(k-1)}]\} - \mathbf{R}\|_2^2$. To solve a single iterate of (4.4), the algorithm utilize an accelerated
 277 alternating minimization method specifically for nonsmooth, nonconvex objectives (iPalm
 278 [40], see appendix). We choose the step size for this method by backtracking since (4.4) can
 279 be highly non-smooth locally.
 280

281 5 Real data experiments

282 Figure 6-(i) compares the reconstruction result ($10\mu\text{m}$ per pixel) between the line probe
 283 and point probe scans on a simplistic three disc samples ($75\mu\text{m}$ radius, platinum). Here,
 284 the point probe tip diameter and the line probe edge thickness are equivalent ($\approx 20\mu\text{m}$),
 285 and the probe moving speed (100ms), the sampling period ($10\mu\text{m}$), and the probe end
 286 material (platinum) are identical as well. Four images are shown here, including the optical
 287 closeup image for the three discs, the line scans, and the reconstruction image of either
 288 point probe or the line probe. In the optical image, the straight arrow represents the probe
 289 sweeping direction, and the angular arrow states sample rotation direction (clockwise) with
 290 angle θ_s . In the reconstructed images, the black circles indicated the ground truth size and
 291 location of the discs derived from the optical image. The reconstruction algorithm is setup

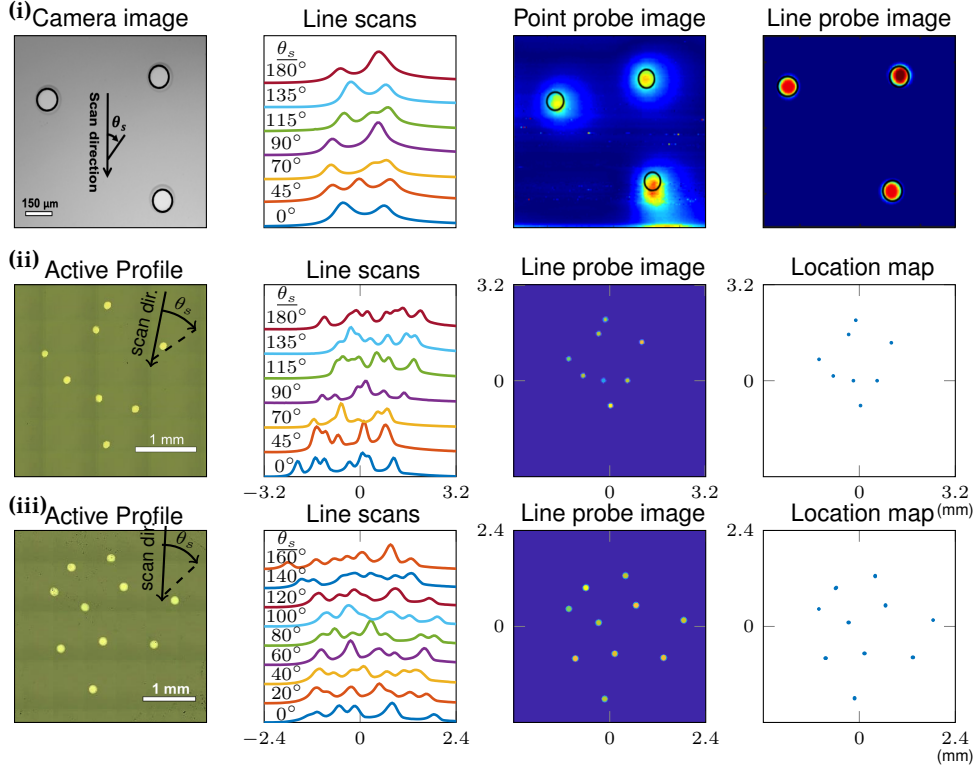


Figure 6: (i). Real data experiments on 3 platinum discs [41], the black circles in the microscopic images are derived from the disc location in camera image. (ii)-(iii). Real data experiments of 8, 10 platinum discs, in which the location map is also the result of line scan reconstruction.

292 with 6 reweighting iterations, where each iterates runs 50 iterates of iPalm. We can see
 293 the reconstruction from point probe exhibits distortion in image due to the skewness of
 294 probe PSF along its proceeding direction during raster scans; while the image of line scan
 295 reconstruction presents three circular features with its size and locations are agreeing with
 296 the ground truth.

297 In Figure 6-(ii)-(iii), we reconstruct the image ($20\mu\text{m}$ per pixel) of samples consist of platinum
 298 discs arranged in a more complicating configuration. Two sets of the experiment are presented here,
 299 which are the samples consist of 8 or 10 discs, while the disc diameter/image
 300 resolution/probe dimension/sampling period/algorithm iterations are all identical to the
 301 three discs case. We demonstrate both of the resulting reconstructed image and the location
 302 map defined by $\mathbf{1}_{\{\mathbf{x}_{ij} \geq 0.5\|\mathbf{x}\|_\infty\}}$ at (i, j) -th entry. For these more complicated images, our
 303 algorithm are still able correctly identify the location and shape of the platinum discs. The
 304 corresponding location maps $\hat{\mathbf{X}}$ are also estimated with reasonable accuracy.

305 6 Summary & Discussion

306 This paper describes issues, both theoretical and practical, that arise in reconstructing images
 307 from a new scanning probe microscopy technique, which has the potential to image sparsely
 308 populated samples much more efficiently than conventional approaches. There are many
 309 directions for future work. Our focus here has been on SECM, but the approach and technical
 310 results here are applicable to other scanning probe microscopy modalities, and are potentially
 311 applicable to other modalities such as CT that image based on projections. Motivated by
 312 materials science applications, our reconstruction approach focuses on images consisting of
 313 localized features; in other areas, different signal models may be approach. Unlike many
 314 other imaging modalities, in SPM the design of probe topography (i.e. the sampling pattern)
 315 is not limited to a straight line, therefore it is possible to adopt various different probe design
 316 accommodate different signal structures. Finally, obtaining sharp estimates of the required
 317 number of line scans is an interesting question for future theoretical work.

References

- [1] R. Wiesendanger and W. Roland, *Scanning probe microscopy and spectroscopy: methods and applications*. Cambridge university press, 1994.
- [2] D. L. Donoho *et al.*, "Compressed sensing," *IEEE Transactions on information theory*, vol. 52, no. 4, pp. 1289–1306, 2006.
- [3] E. J. Candès and M. B. Wakin, "An introduction to compressive sampling [a sensing/sampling paradigm that goes against the common knowledge in data acquisition]," *IEEE signal processing magazine*, vol. 25, no. 2, pp. 21–30, 2008.
- [4] S. Foucart and H. Rauhut, "A mathematical introduction to compressive sensing," *Bull. Am. Math*, vol. 54, pp. 151–165, 2017.
- [5] M. Lustig, D. L. Donoho, J. M. Santos, and J. M. Pauly, "Compressed sensing mri," *IEEE signal processing magazine*, vol. 25, no. 2, p. 72, 2008.
- [6] V. Studer, J. Bobin, M. Chahid, H. S. Mousavi, E. Candes, and M. Dahan, "Compressive fluorescence microscopy for biological and hyperspectral imaging," *Proceedings of the National Academy of Sciences*, vol. 109, no. 26, pp. E1679–E1687, 2012.
- [7] A. Veeraraghavan, D. Reddy, and R. Raskar, "Coded strobing photography: Compressive sensing of high speed periodic videos," *IEEE Transactions on Pattern Analysis and Machine Intelligence*, vol. 33, no. 4, pp. 671–686, 2011.
- [8] G. D. O'Neil, H.-W. Kuo, D. N. Lomax, J. Wright, and D. V. Esposito, "Scanning line probe microscopy: Beyond the point probe," *Analytical chemistry*, vol. 90, no. 19, pp. 11 531–11 537, 2018.
- [9] A. J. Bard, L. R. Faulkner, J. Leddy, and C. G. Zoski, *Electrochemical methods: fundamentals and applications*. Wiley New York, 1980, vol. 2.
- [10] A. J. Bard, F.-R. F. Fan, D. T. Pierce, P. R. Unwin, D. O. Wipf, and F. Zhou, "Chemical imaging of surfaces with the scanning electrochemical microscope," *Science*, vol. 254, no. 5028, pp. 68–74, 1991.
- [11] G. N. Hounsfield, "Computerized transverse axial scanning (tomography): Part 1. description of system," *The British journal of radiology*, vol. 46, no. 552, pp. 1016–1022, 1973.
- [12] A. C. Kak, "Computerized tomography with x-ray, emission, and ultrasound sources," *Proceedings of the IEEE*, vol. 67, no. 9, pp. 1245–1272, 1979.
- [13] G. T. Herman, *Fundamentals of computerized tomography: image reconstruction from projections*. Springer Science & Business Media, 2009.
- [14] S. L. Wellington, H. J. Vinegar *et al.*, "X-ray computerized tomography," *Journal of Petroleum Technology*, vol. 39, no. 08, pp. 885–898, 1987.
- [15] N. Duric, P. Littrup, A. Babkin, D. Chambers, S. Azevedo, A. Kalinin, R. Pevzner, M. Tokarev, E. Holsapple, O. Rama *et al.*, "Development of ultrasound tomography for breast imaging: Technical assessment," *Medical Physics*, vol. 32, no. 5, pp. 1375–1386, 2005.
- [16] J. Frank, *Electron tomography*. Springer, 1992.
- [17] J. Nuyts, B. De Man, P. Dupont, M. Defrise, P. Suetens, and L. Mortelmans, "Iterative reconstruction for helical ct: a simulation study," *Physics in Medicine & Biology*, vol. 43, no. 4, p. 729, 1998.
- [18] L. A. Shepp and B. F. Logan, "The fourier reconstruction of a head section," *IEEE Transactions on nuclear science*, vol. 21, no. 3, pp. 21–43, 1974.
- [19] G.-H. Chen, J. Tang, and S. Leng, "Prior image constrained compressed sensing (piccs): a method to accurately reconstruct dynamic ct images from highly undersampled projection data sets," *Medical physics*, vol. 35, no. 2, pp. 660–663, 2008.
- [20] K. Malczewski, "Pet image reconstruction using compressed sensing," in *2013 Signal Processing: Algorithms, Architectures, Arrangements, and Applications (SPA)*. IEEE, 2013, pp. 176–181.
- [21] B. Goris, S. Bals, W. Van den Broek, E. Carbó-Argibay, S. Gómez-Graña, L. M. Liz-Marzán, and G. Van Tendeloo, "Atomic-scale determination of surface facets in gold nanorods," *Nature materials*, vol. 11, no. 11, p. 930, 2012.
- [22] Z. Saghi, D. J. Holland, R. Leary, A. Falqui, G. Bertoni, A. J. Sederman, L. F. Gladden, and P. A. Midgley, "Three-dimensional morphology of iron oxide nanoparticles with reactive concave surfaces. a compressed sensing-electron tomography (cs-et) approach," *Nano letters*, vol. 11, no. 11, pp. 4666–4673, 2011.
- [23] R. Leary, Z. Saghi, P. A. Midgley, and D. J. Holland, "Compressed sensing electron tomography," *Ultramicroscopy*, vol. 131, pp. 70–91, 2013.

- 373 [24] L. Donati, M. Nilchian, S. Trépout, C. Messaoudi, S. Marco, and M. Unser, "Compressed sensing
374 for stem tomography," *Ultramicroscopy*, vol. 179, pp. 47–56, 2017.
- 375 [25] P. Binev, W. Dahmen, R. DeVore, P. Lamby, D. Savu, and R. Sharples, "Compressed sensing and
376 electron microscopy," in *Modeling Nanoscale Imaging in Electron Microscopy*. Springer, 2012, pp.
377 73–126.
- 378 [26] O. Nicoletti, F. de La Peña, R. K. Leary, D. J. Holland, C. Ducati, and P. A. Midgley, "Three-
379 dimensional imaging of localized surface plasmon resonances of metal nanoparticles," *Nature*,
380 vol. 502, no. 7469, p. 80, 2013.
- 381 [27] M. E. Davis, J. E. Zuckerman, C. H. J. Choi, D. Seligson, A. Tolcher, C. A. Alabi, Y. Yen, J. D. Heide,
382 and A. Ribas, "Evidence of rna in humans from systemically administered sirna via targeted
383 nanoparticles," *Nature*, vol. 464, no. 7291, p. 1067, 2010.
- 384 [28] C. A. S. Batista, R. G. Larson, and N. A. Kotov, "Nonadditivity of nanoparticle interactions,"
385 *Science*, vol. 350, no. 6257, p. 1242477, 2015.
- 386 [29] S. C. Cheung, J. Y. Shin, Y. Lau, Z. Chen, J. Sun, Y. Zhang, J. N. Wright, and A. N. Pasupa-
387 thy, "Dictionary learning in fourier transform scanning tunneling spectroscopy," *arXiv preprint*
388 *arXiv:1807.10752*, 2018.
- 389 [30] J. Radon, "1.1 über die bestimmung von funktionen durch ihre integralwerte längs gewisser
390 mannigfaltigkeiten," *Classic papers in modern diagnostic radiology*, vol. 5, p. 21, 2005.
- 391 [31] A. M. Cormack, "Representation of a function by its line integrals, with some radiological appli-
392 cations," *Journal of applied physics*, vol. 34, no. 9, pp. 2722–2727, 1963.
- 393 [32] F. Natterer, *The Mathematics of Computerized Tomography*. Philadelphia, PA, USA: Society for
394 Industrial and Applied Mathematics, 2001.
- 395 [33] S. Helgason, *Integral geometry and Radon transforms*. Springer Science & Business Media, 2010.
- 396 [34] S. Farsiu, D. Robinson, M. Elad, and P. Milanfar, "Advances and challenges in super-resolution,"
397 *International Journal of Imaging Systems and Technology*, vol. 14, no. 2, pp. 47–57, 2004.
- 398 [35] E. J. Candès and C. Fernandez-Granda, "Towards a mathematical theory of super-resolution,"
399 *Communications on Pure and Applied Mathematics*, vol. 67, no. 6, pp. 906–956, 2014.
- 400 [36] D. L. Donoho, M. Elad, and V. N. Temlyakov, "Stable recovery of sparse overcomplete represen-
401 tations in the presence of noise," *IEEE Transactions on information theory*, vol. 52, no. 1, pp. 6–18,
402 2006.
- 403 [37] E. Candès and T. Tao, "Decoding by linear programming," *arXiv preprint math/0502327*, 2005.
- 404 [38] K. G. Larkin, M. A. Oldfield, and H. Klemm, "Fast fourier method for the accurate rotation of
405 sampled images," *Optics communications*, vol. 139, no. 1-3, pp. 99–106, 1997.
- 406 [39] E. J. Candès, M. B. Wakin, and S. P. Boyd, "Enhancing sparsity by reweighted l1 minimization,"
407 *Journal of Fourier analysis and applications*, vol. 14, no. 5-6, pp. 877–905, 2008.
- 408 [40] T. Pock and S. Sabach, "Inertial proximal alternating linearized minimization (ipalm) for non-
409 convex and nonsmooth problems," *SIAM Journal on Imaging Sciences*, vol. 9, no. 4, pp. 1756–1787,
410 2016.
- 411 [41] A. E. Dorfi, H.-W. Kuo, V. Smirnova, J. Wright, and D. V. Esposito, "Design and operation of
412 a scanning electrochemical microscope for imaging with continuous line probes," *Manuscript*
413 *submitted under review*, 2019.